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<p>(21) International Application Number: PCT/GB89/00320 (22) International Filing Date: 28 March 1989 (28.03.89)</p> <p>(31) Priority Application Number: 8807488.5 (32) Priority Date: 29 March 1988 (29.03.88) (33) Priority Country: GB</p> <p>(71) Applicant (<i>for all designated States except US</i>): ARES-SERONO RESEARCH & DEVELOPMENT LIMITED PARTNERSHIP [US/US]; Exchange Place, 37th Floor, Boston, MA 02109 (US).</p> <p>(72) Inventors; and (75) Inventors/Applicants (<i>for US only</i>) : FLANAGAN, Michael, Thomas [GB/GB]; 17 Chinnery Hill, Bishop's Stortford, Hertfordshire CM23 3PS (GB). ASHWORTH, Robert, Heddle [GB/GB]; 18 Downshire Hill, Hampstead, London NW3 1NT (GB).</p>		<p>(74) Agent: FRANK B DEHN & CO.; Imperial House, 15-19 Kingsway, London WC2B 6UZ (GB).</p> <p>(81) Designated States: AT (European patent), AU, BE (European patent), CH (European patent), DE (European patent), FR (European patent), GB (European patent), IT (European patent), JP, LU (European patent), NL (European patent), NO, SE (European patent), US.</p> <p>Published <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i></p>	
<p>(54) Title: METHOD OF ASSAY</p> <p>(57) Abstract</p> <p>Assay techniques are described which employ the evanescent field properties of optical waveguides combined with a resonance energy transfer step between fluorophores bound to reagents involved in the assay. Also described are a kit and a device for use in such assays.</p>			

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Method of Assay

This invention relates to assay techniques and to means for putting such techniques into effect. In particular it relates to an improved assay technique providing an enhanced signal-to-noise ratio and enhanced 5 sensitivity.

Fluorescence assays, for example fluorescence immunoassays, where one component of the assay is immobilised on a waveguide interface, give rise to the problem of differentiating between fluorescence 10 emission from a labelled further assay reagent that is bound to the surface (the required signal) and fluorescence emission from that further reagent which is still in solution giving unwanted noise signal.

A greater differentiation between these two 15 populations of bound and unbound reagent would improve the signal-to-noise ratio and sensitivity of the assay.

The invention described below makes use of the evanescent field properties of optical waveguides 20 combined with a resonance energy transfer step [Forster Energy Transfer; cf. Th. Forster, Ann. Phys. 2, 55- 75 (1958)] between a fluorophore bound to a reagent X, on or near an immobilised detection reagent Y, for example an antibody, and in some cases, dyes 25 immobilised on the waveguide, within the waveguide, or within an immobilised film support.

The differentiation between bound and free reagents in homogeneous assays of the type achieved because energy transfer will only occur efficiently 30 across molecular dimensions and hence will be observed only on complex formation.

Known evanescent waveguide assays are based on the assumption that the penetration of the evanescent

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wave is negligible beyond molecular dimensions and hence only excites the label on the complex. However, in reality, this assumption is an oversimplification and the sensitivity of such assays is less than might 5 be expected.

According to one aspect of the present invention there is provided a method of assay of a ligand in a sample which comprises

(A) incubating, simultaneously or in any desired 10 sequence,

- (a) the sample,
- (b) a reagent X labelled with a first energy acceptor,
- (c) a reagent Y immobilised directly or indirectly 15 on the surface of an optical waveguide,
- (d) a second energy acceptor immobilised directly or indirectly (if desired via reagent Y) on the surface of the optical waveguide, or immobilised within the said waveguide,
- (e) if desired, at least one further energy acceptor, 20 which may be the same as or different from said first or second energy acceptors, immobilised directly or indirectly on or within the surface of said optical waveguide, wherein one of the reagents X and Y comprises a specific binding 25 partner to said ligand and the other reagents X and Y comprises either a ligand analogue or a specific binding partner of said ligand and wherein one of the said first and second energy acceptors comprises a fluorophore (a "donor fluorophore") the electronic emission 30 spectrum of which overlaps with the electronic absorption spectrum of the other of said first and second energy acceptors;

(B) irradiating the said optical waveguide with 35 electromagnetic radiation of a wavelength suitable for exciting said donor fluorophore; and

(C) detecting whether and, if desired, the extend to which and/or rate at which, resonance energy transfer

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occurs, either directly or indirectly, between the first and second energy acceptors or between the second and first energy acceptors respectively: wherein either the irradiation of step (B) is by means of
5 the evanescent field produced by electromagnetic radiation propagating along said waveguide and/or the detection step (C) utilises evanescent field coupling into the waveguide of the fluorescence of the first energy acceptor or the fluorescence, if
10 any, of the second energy acceptor.

The term "ligand analogue" as used herein refers to a species capable of complexing with the same binding site of the same specific binding partner as the ligand under assay, and includes inter alia
15 within its scope a known quantity of the ligand under assay.

The term "energy acceptor" as used herein denotes a compound which is capable of absorbing electromagnetic energy, for example, a dye or a fluorophore. Typical
20 energy acceptors include, for example, those of the coumarin, fluorescein, lucifer yellow and rhodamine families, phycobiliproteins and erythrosin: specific examples of energy acceptors include fluorescein isothiocyanate, rhodamine B, rhodamine 6G, rhodamine 25 123, R-phycoerythrin, c-phycocyanin, allophycocyanin, fluorescamine, lucifer yellow VS and lucifer yellow CH. As mentioned above, one of the said first and second energy acceptors is a donor fluorophore.
The other of the said first and second energy acceptors
30 may be an acceptor fluorophore or an acceptor dye. The energy acceptors are chosen such that excitation of the donor fluorophore by electromagnetic radiation of a suitable wavelength and formation of a direct or indirect complex between reagents X and Y facilitates
35 resonance energy transfer, either directly or indirectly, between the energy acceptors. Thus, when the first and second energy acceptors comprise a donor fluorophore

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and an acceptor dye or an acceptor dye and a donor fluorophore respectively, the fluorescence of the donor fluorophore is quenched and when the first and second energy acceptors comprise a donor fluorophore 5 and an acceptor fluorophore or an acceptor fluorophore and a donor fluorophore respectively, the fluorescence of the donor fluorophore is quenched and the acceptor fluorophore fluoresces (although the fluorescence of the acceptor fluorophore may have a very low quantum 10 efficiency).

By way of example only, representative pairs of compounds which are suitable for use as donor and acceptor fluorophores in the invention are listed in Table 1 below.

15

Table 1

	Donor fluorophore	Corresponding acceptor fluorophore
20	fluorescein isothiocyanate	rhodamine B
	R-phycoerythrin	allophycocyanin
	fluorescein isothiocyanate	R-phycoerythrin
	rhodamine B	allophycocyanin
25	fluorescamine	lucifer yellow VS.
	c-phyccocyanin	R-phycoerythrin

When at least one further energy acceptor is present as component (e) two or more resonance energy transfer steps may occur. Thus, for example, when 30 the first energy acceptor is an acceptor dye, the second energy acceptor is a donor fluorophore and an acceptor fluorophore is present as component (e), complex formation between reagents X and Y facilitates 35 resonance energy transfer between the donor fluorophore

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and the acceptor dye such that the acceptor dye quenches the fluorescence emitted by both the donor fluorophore and the acceptor fluorophore present as component (e).

By detecting whether resonance energy transfer 5 between the first and second energy acceptors or vice versa occurs, it may be possible to detect the quenching of the fluorescence of the donor fluorophore and/or, when present, the fluorescence of an acceptor fluorophore. When one or more further energy acceptors 10 are present as component (e) the quenching and/or fluorescence of one or more components may be detected. Thus, for example, when the first energy acceptor is an acceptor dye, the second energy acceptor is a donor fluorophore and an acceptor fluorophore is 15 present as component (e) quenching of the fluorescence of the donor fluorophore and/or the acceptor fluorophore may be detected.

Where one of reagents X and Y comprises a ligand analogue and the other of reagents X and Y comprises 20 a specific binding partner to the ligand, complex formation between reagents X and Y may occur directly. Alternatively, where both reagents X and Y comprise specific binding partners to the ligand, complex formation between reagents X and Y indirectly via 25 the ligand, if present in the sample, may occur.

It is to be understood that reagent Y may be immobilised on the surface of the optical waveguide either directly or indirectly. For example, when reagent Y is an antibody, indirect immobilisation 30 may be effected by means of an anti-species antibody to reagent Y which is itself bound to the surface of the optical waveguide.

Immobilization on the surface of the optical waveguide may thus occur by means of immunological 35 bonding as in an antibody-antigen or antibody-hapten bond or non-immunological bonding such as that between

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a protein and a ligand, e.g. between avidin and biotin.

Suitable materials for the optical waveguide include, for example, glass (e.g. permabloc glass or crown glass), plastics (e.g. acrylic or polystyrene),
5 silica and quartz; but in principle any material of suitable refractive index may be used which is transparent to radiation at least at the wavelengths involved in the assay.

Preferably both the irradiation step (B) and
10 the detection step (C) utilise evanescent-field coupling.

Several advantages arise by combining the two techniques of resonance energy transfer and evanescent-field coupling.

1. The convolution of the inverse sixth power dependence on distance of resonance transfer with the exponential decay of the evanescent wave restricts the localization of the excitation region closer to the waveguide.
15
2. The Stokes shift in frequency between the exciting electromagnetic radiation and the emitted light is increased by a suitable choice of donor fluorophore and, if present, the acceptor fluorophore, thus allowing more effective filtering of the signal.
20
3. The signal-to-noise ratio is improved. When an acceptor fluorophore is present the measurement of the acceptor fluorescence signal in the presence of donor background is facilitated by immobilization of the acceptor on the waveguide surface. The number of transfer pathways can be increased by immobilizing further donors or acceptors on or within the waveguide surface.
25
4. The Stokes shift can be further increased by the coimmobilization of additional fluorophore species, emitting at longer wavelengths, which will allow a chain of transfer steps to occur. Such a chain of transfer steps and an increased
30
35

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number of transfer pathways cannot be effectively incorporated within a conventional homogeneous assay.

5. Transfer along a chain of fluorophores will be more efficient if the immobilised fluorophores are appropriately aligned. Such alignments can be achieved with liquid crystal and Langmuir-Blodgett film deposition in combination with the fluorophore immobilization.
- 10 The optical waveguide mentioned hereinbefore may optionally be incorporated in a grating arrangement such as is described in our copending application of even date (corresponding to British Patent Application 8807486.9) entitled "Waveguide Sensor". Such a grating arrangement, used in combination with the above transfer techniques, will allow the separation and filtering of the emitted and exciting radiation within the waveguiding sensor device itself, removing the need for external monochromators or filters.
- 15 20 It is especially to be noted that devices of the type described and claimed in EP-A-171148 may be advantageously adapted to carry the test samples to be assayed in the method of the present invention. The emitted radiation may be filtered and/or collimated, if desired, before being detected by conventional means, for example one or more photomultiplier tubes.
- 25 According to another aspect of the invention there is provided a kit for carrying out a method 30 of assay as described herein which comprises (i) a reagent X as defined above and (ii) an optical waveguide on the surface of which is immobilised (directly or indirectly) a reagent Y as defined above and on or within which optical waveguide is immobilised (directly or indirectly, if desired via reagent Y) at least one further energy acceptor as defined above.
- 35 According to a further aspect of the invention

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there is provided a device for use in a method of assay as described hereinbefore which comprises an optical waveguide on the surface of which is immobilised (directly or indirectly) either a specific binding 5 partner for the ligand under assay or a ligand analogue, and within which is immobilised a fluorophore or a dye.

The invention will be particularly described hereinafter with reference to an antigen as the ligand 10 and where reagents X and Y each comprise an antibody i.e. a sandwich-type immunoassay. However, the invention is also applicable to competition-type immunoassays, for example where one of reagents X and Y comprises an antibody and the other comprises a ligand analogue.

15 Furthermore, the invention is not to be taken as limited to assays of antibodies or antigens.

Examples of ligands which may be assayed by the method of the invention are given in Table 2 below, together with an indication of a suitable specific binding 20 partner in each instance.

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Table 2

Ligand	Specific Binding Partner
5 antigen	specific antibody
antibody	antigen
hormone	hormone receptor
hormone receptor	hormone
polynucleotide strand	complementary polynucleotide strand
10 avidin	biotin
biotin	avidin
protein A	immunoglobulin
immunoglobulin	protein A
15 enzyme	enzyme cofactor (substrate) or inhibitor
enzyme cofactor (substrate) or inhibitor	enzyme
lectins	specific carbohydrate
20 specific carbohydrate of lectins	lectins

The method of the invention has very broad applicability but in particular may be used to assay:

25 hormones, including peptide hormones (e.g. thyroid stimulating hormone (TSH), luteinising hormone (LH), human chorionic gonadotrophin (hCG), follicle stimulating hormone (FSH), insulin and prolactin) or non-peptide hormones (e.g. steroid hormones such as cortisol, estradiol, progesterone and testosterone, or thyroid hormones such as thyroxine (T4) and triiodothyronine), proteins (e.g. carcinoembryonic antigen (CEA) and alphafetoprotein (AFP)), drugs (e.g. digoxin), sugars, toxins, vitamins, viruses such as influenza, para-influenza, adeno-, hepatitis, respiratory and AIDS viruses, or microorganisms.

It will be understood that the term "antibody"

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used herein includes within its scope:

- (a) any of the various classes or sub-classes of immunoglobulin, e.g. IgG, IgM, derived from any of the animals conventionally used, e.g. sheep, rabbits, goats or mice,
- 5 (b) monoclonal antibodies,
- (c) intact molecules or "fragments" of antibodies, monoclonal or polyclonal, the fragments being those which contain the binding region of the antibody, i.e. fragments devoid of the Fc portion (e.g. Fab, Fab', F(ab')₂) or the so-called "half-molecule" fragments obtained by reductive cleavage of the disulphide bonds connecting the heavy chain components in the intact antibody.
- 10
- 15 The method of preparation of fragments of antibodies is well known in the art and will not be described herein.

The term "antigen" as used herein will be understood to include both permanently antigenic species (for example, proteins, bacteria, bacterial fragments, 20 cells, cell fragments and viruses) and haptens which may be rendered antigenic under suitable conditions.

For a better understanding of the present invention, reference is made to the accompanying drawings wherein 25 Figures 1 to 10 depict schematically various assay formats according to the invention and Figure 11 shows schematically an arrangement of apparatus which is suitable for carrying out the method of the invention.

In the embodiments depicted in the drawings 30 Forster energy transfer occurs from an excited "donor" fluorophore (D) to an "acceptor" fluorophore (A). The donor fluorophore is excited either by an evanescent field of light guided within the waveguide to which the assay complex is immobilised or directly by light 35 from above or below the waveguide.

Fluorescent emission is collected from both, or either, of the donor and acceptor fluorophores.

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The fluorescent emission is either coupled into waveguide modes or (when the donor fluorophore is excited by an evanescent field of light) may be transmitted across the waveguide prior to detection.

5 Fig. 1 shows the surface 2 of an optical waveguide with an antibody 4 (reagent Y) immobilised thereon, which antibody is labelled with an acceptor fluorophore (A). A second antibody 6, labelled with a donor fluorophore (D) is present as reagent X.

10 During the assay, an antigen 8 (i.e. the ligand) in the sample becomes bound to binding sites both on the A-labelled antibody 4 and on the D-labelled antibody 6, thereby forming a "sandwich complex". The donor fluorophore D is electronically excited
15 by absorption of incident radiation. Forster energy transfer 10 then occurs between the donor fluorophore D and the acceptor fluorophore A, causing the latter to become electronically excited, whilst the donor fluorophore is deactivated and so loses its ability
20 to fluoresce. During the assay, the fluorescence from either or both fluorophores may be monitored.

In a further embodiment of the invention shown in Fig. 2 the immobilised reagent Y is the Fab fragment 12 of an antibody. The use of such fragments reduces
25 the distance between the donor and the acceptor fluorophores and hence makes energy transfer more efficient.

In this embodiment, acceptor fluorophores 14 are immobilised on the surface of the optical waveguide.

Fig. 3 shows the reverse of the situation shown
30 in Fig. 1. The immobilised antibody 22 (reagent Y) is labelled with a donor fluorophore (D) and reagent X comprises a second antibody 24 labelled with an acceptor fluorophore (A).

If the acceptor fluorophore has a very low
35 quantum yield of fluorescence it may be preferable to detect the quenching of the donor fluorescent emission intensity rather than detecting an increase

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from zero intensity of the emission from the fluorescent acceptor. An acceptor dye provides a limiting case of an acceptor fluorophore the fluorescence quantum yield of which is negligibly small

5 Fig. 4 shows a waveguide surface on which are immobilised an acceptor fluorophore (A) and an antibody 34 labelled with the same type of acceptor fluorophore (A). This arrangement increases the efficiency of energy transfer from the donor fluorophore (D)

10 by reducing the distance between donor and acceptor and increasing the number of transfer pathways.

In Fig. 5, in addition to an immobilised antibody 40 labelled with acceptor fluorophore and the immobilised acceptor fluorophore as in Fig. 4, a polymer layer 42 is also immobilised onto the waveguide surface. This polymer layer may also be labelled with an acceptor fluorophore (A) 44 and this serves to reduce the average distance between the donor and acceptor fluorophores. An appropriate choice

15 of polymer will also reduce the amount of non-specific binding of the donor fluorophore (D) - labelled antibody 46 to the waveguide surface, which would give unwanted noise signal.

Alternatively, the acceptor fluorophore may

20 be absorbed within the waveguide surface as shown in Fig. 6. This avoids the loss of fluorescence emission on transmission through the upper waveguide interface.

Fig. 7 shows an embodiment similar to that

25 of Fig. 6 except that the positions of the donor and acceptor fluorophores are reversed.

Fig. 8 shows an immobilised molecular matrix which both incorporates acceptor fluorophores and aligns them. This serves to change the angular profile

30 of acceptor fluorescence emission in order to improve the efficiency with which it is collected by the collimation and detection system. If the donor and

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acceptor positions are exchanged then efficient excitation of the donor can be arranged as shown in Fig. 9.

In a further embodiment of the invention, shown in Fig. 10, the binding of an antibody 52 labelled 5 with an energy acceptor which does not fluoresce e.g. a dye (A2) will reduce the transfer of energy from a donor fluorophore (D) to an acceptor fluorophore (A1). This combines the detection of quenching of A1 with an improved Stokes shift introduced by the 10 energy transfer step.

In each of the embodiments depicted in Figs. 4 to 10 an enhanced Stokes shift separation between exciting and emission wavelengths can be achieved by coimmobilization of more than one donor or acceptor species 15 at the waveguide surface, on the polymer, or within the aligning matrix. The aligning matrix may itself be fluorescent. The enhancement results from the successive transfer from one fluorescent species to the next.

Fig. 11 shows an experimental set-up suitable 20 for carrying out an assay in accordance with the method of the invention. Radiation of a wavelength suitable for the assay emerges from a light source 62 and, after collimation by a conventional system 25 of lenses, passes through a slit 63 and a filter 64. The resulting beam of radiation 65 is chopped by a chopper 66 and then split by means of a beam splitter 67: the reflected part of the beam (the reference beam) passes into a photomultiplier tube 30 68, via a neutral density filter 69; the transmitted part of the beam passes through a hemicylindrical prism 70 and into a waveguide 71 which is attached to the prism by means of a transparent index-matching fluid or glue. In this example, sample liquid is 35 drawn into a capillary cavity between the waveguide 71 and an upper plate 72, as would be found, for example, in a capillary fill device (see, for example,

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EP-A-171148). Light which emerges from the prism 70 is detected by one or more than one photomultiplier tube 73 after passing through one or more than one suitable filter 74. The photomultiplier tubes 68 5 and 73 and the chopper 66 are integrated by means of a lock-in amplifier 75. The signals from the photomultiplier tubes may be processed and output as desired.

The following non-limiting Example illustrates 10 the present invention.

Example 1

Assay of Human Chorionic Gonadotrophin (hCG)

15 In this assay, fluorescently labelled antibody becomes bound as a result of formation of a sandwich complex with the analyte ligand (hCG) and a second antibody, also labelled with fluorophore, which is linked to the waveguide.

20 Preparation of Starting Materials

(i) Fabrication of avidin-coated waveguides

Glass waveguides, 10 x 20 x 1.1 mm, were cut out of Permabloc glass (Pilkington Glass Ltd., St. 25 Helens, UK) using standard glass scribing techniques. After thorough washing with detergent and ultrasonic agitation, the glass was activated with a silane (8% 3-glycidoxypropyl-trimethoxysilane (Fluka, Glossop, UK)) at pH 3.5 for 2 hours. The glass was then washed 30 and an appropriate cross-linking agent (e.g. SMCC; succinimidyl 4-(N-maleimidomethyl)cyclohexane-1-carboxylate (Pierce, Luton, England) or glutaraldehyde) was used to couple avidin to the glass surface using standard techniques (see, for example, Ishikura et al, Journal 35 of Immunoassay 4, 209-237(1983)). The glass slides were then spin-coated with 10% sucrose solution containing

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0.1% casein and stored dry at 4°C until use.

(ii) Preparation of biotin/R-phycoerythrin/anti-hCG antibody

Monoclonal anti-hCG antibodies were obtained
5 from mouse ascites fluid by the method of Milstein
and Kohler in Nature 256, 495-497 (1975). Antibodies
from individual hybridoma cell lines were screened
to identify those producing antibody to discrete
antigen determinants. Those having the highest affinities
10 to hCG were selected for use in the assay. 1.48
mg R-phycoerythrin was mixed with 0.34 mg N-hydroxy-
succinimido-biotin ester (Sigma, Poole, UK) using
standard methods (see Guesdon et al, J. Histochem.
Cytochem. 27, 1131 (1979)). The resulting phycoery-
15 thrin/biotin conjugate was purified using a Pharmacia
PD10 column employing 0.2 M sodium bicarbonate buffer,
pH 9.0 then activated with SMCC (see Ishikura et
al, Journal of Immunoassay 4 209-327 (1983)). Antibody
A was activated with 2-iminothiolane and then mixed
20 with the phycoerythrin/biotin conjugate in equal
amounts and left overnight at 4°C. The conjugate
is purified on a TSK 3000 SWG column eluted with
a triethanolamine buffer (0.1 M, pH 7.3) containing
NaCl (0.1 M), MgCl₂ (10⁻³ M), ZnCl₂ (10⁻³ M) and 1%
25 NaN₃, the fractions of highest-molecular weight being
collected.

(iii) Preparation of allophycocyanin/anti-hCG antibody

Antibody B (a second monoclonal antibody to
hCG, specific for a different antigenic determinant)
30 was conjugated to allophycocyanin following methods
outlined in Stryer et al, US 4,542,104(1985).

(iv) Preparation of hCG standard solutions

A freeze-dried preparation of hCG, calibrated
against the first international reference preparation

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(75/537) was obtained from Biodata SpA, Milan, Italy. This sample was diluted in horse serum (Serono Diagnostics, Woking, England) to the desired concentration.

5 Apparatus for optical measurements

An optical apparatus suitable for conducting an assay according to the present invention is shown in figure 11 of the accompanying drawings. The light source 62 is a 150 W xenon arc lamp, the excitation filter 64 has a centre wavelength of 485 nm (60 nm bandwidth), the detection filter has a centre wavelength of 580 nm (70 nm bandwidth). These filters are suitable for an assay involving R-phycoerythrin. A long-pass collector for allophycocyanin had a cut-on at 645 nm. A Hakuto R928 photomultiplier tube (Hakuto, Waltham Cross UK) is employed as the photodetectors 68 & 73 and an EG and G 5207 (PAR, Prenton, USA) lock-in amplifier 75 is employed. The glass waveguide 71 may be mounted in a cell of sufficiently small dimensions so as to allow the sample to be drawn over the waveguide surface via capillary action.

Assay procedure

A sandwich assay utilizing the above starting materials and apparatus may be carried out as follows:

The avidin-coated waveguide is incubated with a solution of the biotin/R-phycoerythrin/anti-hCG antibody. The donor fluorophore-labelled antibody A is thus immobilised on the waveguide surface as a result of the high mutual affinity of avidin and biotin. The waveguide is then incubated with sample containing the antigen under assay (hCG) and a fixed amount of the allophycocyanin(acceptor fluorophore)-labelled antibody B. The waveguide is illuminated with radiation at a wavelength suitable for excitation of the donor fluorophore, i.e. around 485 nm for R-phycoerythrin. This illumination may be effected

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either after equilibrium has been attached or during the course of the attainment of equilibrium. The intensity of light emitted from the donor fluorophore is monitored, i.e. around 580 nm for R-phycoerythrin.

- 5 As a result of formation of sandwich complex, the fluorescence intensity at 580 nm will decrease as a function of the concentration of hCG. Calibration may be effected by comparison of results with sample solutions containing zero or known amounts of hCG.
- 10 As mentioned above, competition-type assays may also be carried out by the method of the invention. The procedure in these cases is similar.

Competition assay for hCG

- 15 Antibody labelled with donor fluorophore (R-phycoerythrin) is immobilised at the waveguide surface by means of the avidin/biotin interaction, according to the method described above. Acceptor fluorophore (allophycocyanin) is conjugated to hCG molecules.
- 20 The waveguide is then incubated with liquid sample containing hCG and a fixed, known amount of allophycocyanin/hCG conjugate. The donor fluorophores are excited by application of light of a suitable wavelength, and the attenuation of the fluorescence of the donor
- 25 fluorophore is monitored. Fluorescence due to the donor fluorophore decrease with decreasing amount of hCG in the sample.

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Claims:

1. A method of assay of a ligand in a sample which comprises
 - (A) incubating, simultaneously or in any desired sequence,
 - 5 (a) the sample,
 - (b) a reagent X labelled with a first energy acceptor,
 - (c) a reagent Y immobilised directly or indirectly on the surface of an optical waveguide,
 - (d) a second energy acceptor immobilised directly
 - 10 or indirectly (if desired via reagent Y) on the surface of the optical waveguide, or immobilised within the said waveguide,
 - (e) if desired, at least one further energy acceptor, which may be the same as or different from
- 15 said first or second energy acceptors, immobilised directly or indirectly on or within the surface of said optical waveguide, wherein one of the reagents X and Y comprises a specific binding partner to said ligand and the other reagents
- 20 X and Y comprises either a ligand analogue or a specific binding partner of said ligand and wherein one of the said first and second energy acceptors comprises a fluorophore (a "donor fluorophore") the electronic emission spectrum of which overlaps with the electronic absorption spectrum of the other of said first and second energy acceptors;
- 25 (B) irradiating the said optical waveguide with electromagnetic radiation of a wavelength suitable for exciting said donor fluorophore; and
- (C) detecting whether and, if desired, the extend to which and/or rate at which, resonance energy transfer occurs, either directly or indirectly, between the first and second energy acceptors or between the
- 30 second and first energy acceptors respectively: wherein

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either the irradiation of step (B) is by means of
the evanescent field produced by electromagnetic
radiation propagating along said waveguide and/or
the detection step (C) utilises evanescent field
5 coupling into the waveguide of the fluorescence of
the first energy acceptor or the fluorescence, if
any, of the second energy acceptor.

2. A method as claimed in claim 1 wherein the
first energy acceptor comprises a donor fluorophore
10 and the second energy acceptor comprises an acceptor
dye or an acceptor fluorophore.

3. A method as claimed in claim 1 wherein the
first energy acceptor comprises an acceptor dye or
an acceptor fluorophore and the second energy acceptor
15 comprises a donor fluorophore.

4. A method as claimed in any one of the preceding
claims wherein an acceptor fluorophore is present
as component (e).

5. A method as claimed in any one of the preceding
20 claims wherein the irradiation step (B) utilizes
the evanescent field associated with the electromagnetic
radiation propagating along the optical waveguide.

6. A method as claimed in any one of the preceding
claims wherein one of the energy acceptors comprises
an acceptor fluorophore and the detection step (C)
25 utilizes evanescent field coupling of the fluorescence
emitted by the acceptor fluorophore into the waveguide.

7. A method as claimed in any one of the preceding
claims wherein the said energy acceptors are selected
from the group comprising phycobiliproteins, coumarins,

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fluorescein, rhodamines, lucifer yellows, erythrosin or derivatives thereof.

8. A method as claimed in claim 1 wherein the optical waveguide is made of glass or silica.

5 9. A kit for use in a method as claimed in claim 1 comprising

(i) a reagent X labelled with a first energy acceptor; and

10 (ii) an optical waveguide on the surface of which is immobilised (directly or indirectly) a reagent Y and on or within which is immobilised (directly, or indirectly, if desired via reagent Y) at least one further energy acceptor,

15 the said reagents X and Y and the said energy acceptors being as defined in claim 1.

10. A device for use in a method as claimed in claim 1 comprising an optical waveguide on the surface of which is immobilised (directly or indirectly) either a specific binding partner for the ligand

20 under assay or a ligand analogue, and within which is immobilised a fluorophore or a dye.

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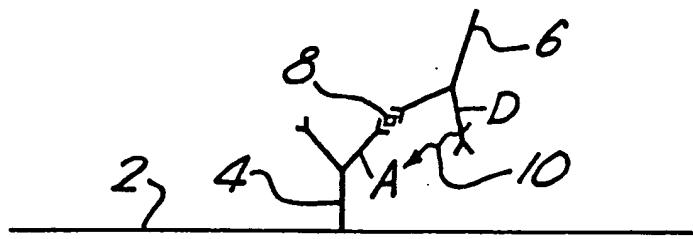


FIG. 1.

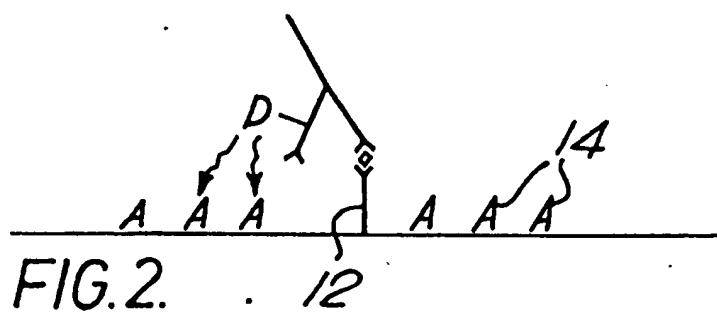


FIG. 2. . 12

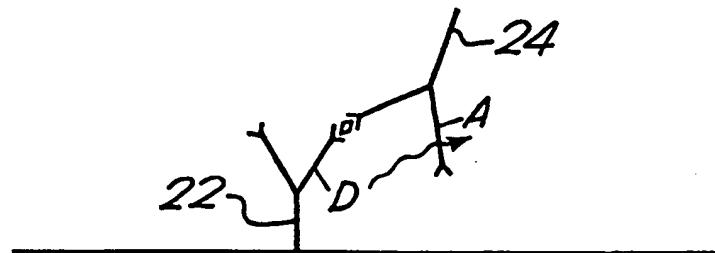


FIG. 3.



FIG. 4.

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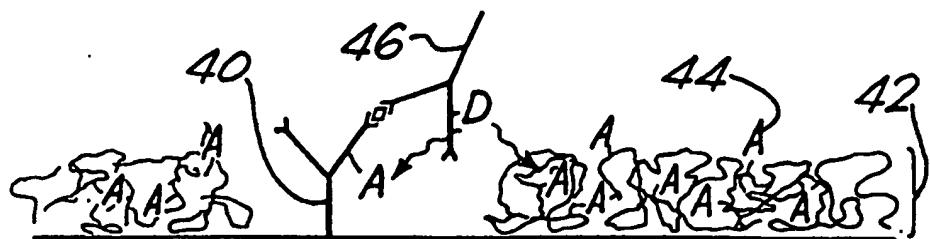


FIG. 5.

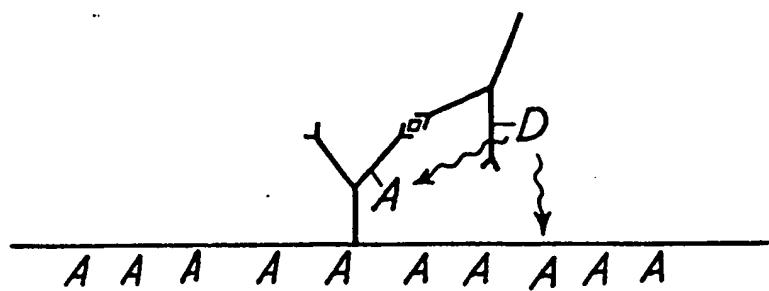


FIG. 6.

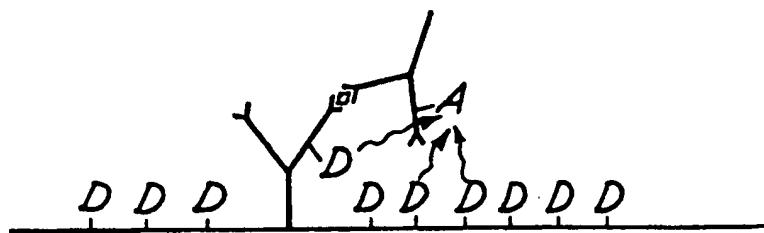


FIG. 7.

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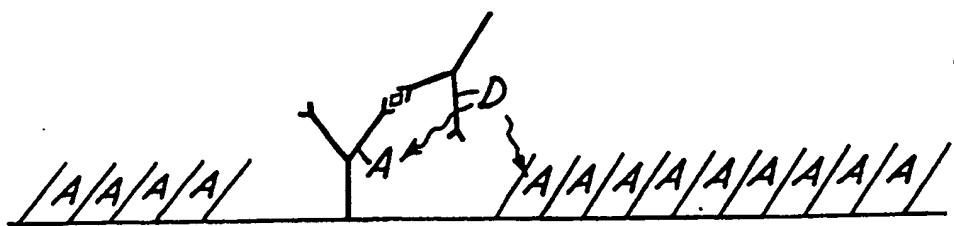


FIG.8.

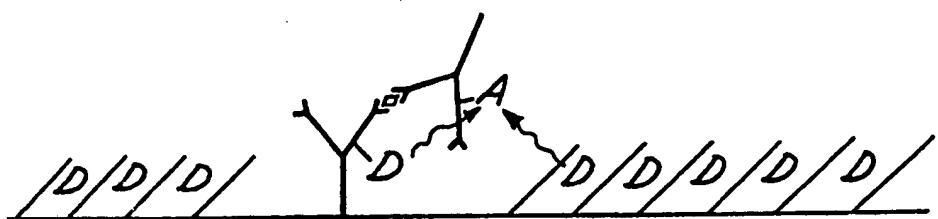


FIG.9.

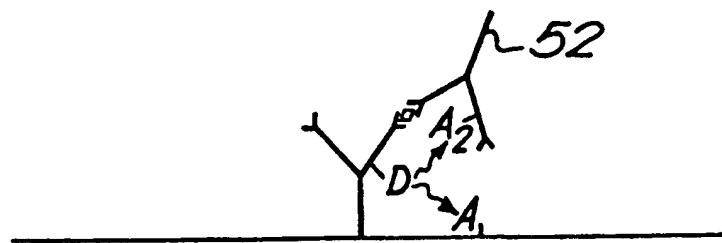


FIG.10.

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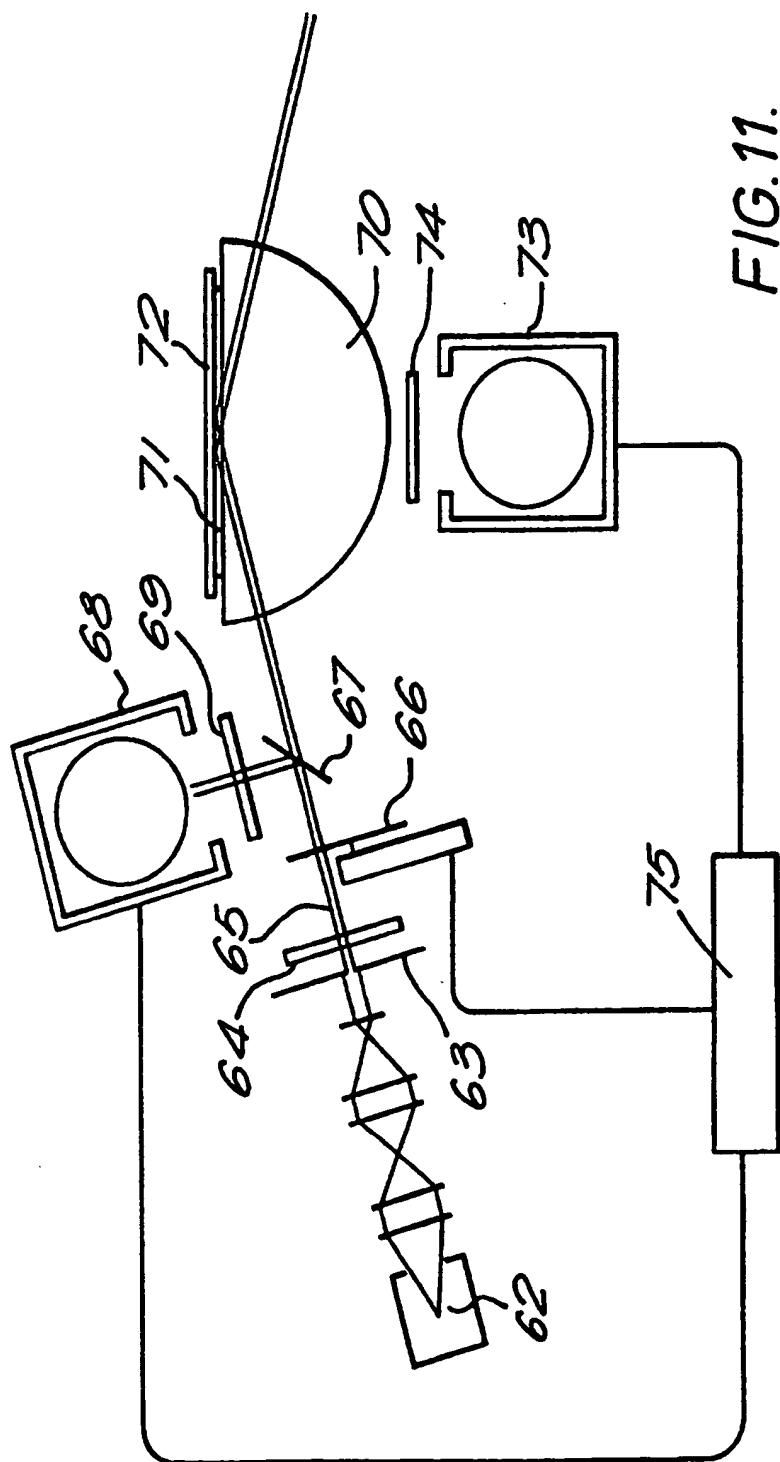


FIG. 11.

INTERNATIONAL SEARCH REPORT

International Application No PCT/GB 89/00320

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) *

According to International Patent Classification (IPC) or to both National Classification and IPC

IPC⁴: G 01 N 33/58, G 01 N 33/552, G 01 N 21/64

II. FIELDS SEARCHED

Minimum Documentation Searched *

Classification System	Classification Symbols
IPC ⁴	G 01 N

Documentation Searched other than Minimum Documentation
to the Extent that such Documents are included in the Fields Searched *

III. DOCUMENTS CONSIDERED TO BE RELEVANT *

Category *	Citation of Document, ** with indication, where appropriate, of the relevant passages ***	Relevant to Claim No. ****
X	EP, A, 0211587 (CORNING GLASS WORKS) 25 February 1987 see column 1, line 1 - column 3, line 58; claims --	1,2,4,5, 8-10
Y	EP, A, 0242527 (ENZO BIOCHEM, INC.) 28 October 1987 see the abstract; page 8, lines 3-7; figure 1; page 11, line 11 - page 14, line 4; page 35, lines 7-32 --	1,2,4-10
Y	EP, A, 0103426 (M.J. BLOCK) 21 March 1984 see the abstract; page 1, line 1 - page 4, line 6; page 11, lines 23-25; page 23, line 13 - page 24, line 27; claims --	1,2,4-10
A	EP, A, 0075353 (BATTELLE MEMORIAL INSTITUTE) 30 March 1983 see page 4, lines 2-24; page 11, line 22 - page 13, line 35; page 30, lines 12-20	1,5-8

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IV. CERTIFICATION

Date of the Actual Completion of the International Search

28th June 1989

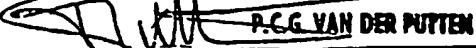
Date of Mailing of this International Search Report

21 JUIL 1989

International Searching Authority

EUROPEAN PATENT OFFICE

Signature of Authorized Officer



P.C.G. VAN DER PUTTEN

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)

Category	Description of Document, with indication, where appropriate, of the relevant passages	Relevant to Claim No.
A	EP, A, 0214768 (THE REGENTS OF THE UNIVERSITY OF CALIFORNIA) 18 March 1987 see page 4, line 24 - page 5, line 16; claims --	1,7
A	Proc. Electrochem. Soc., volume 87-9, (Proc. Symp. Chem. Sens.), 1987, A.L. Harmer: "Guided-wave chemical sensors", pages 409-427 see page 416, line 32 - page 419, last line -----	1

ANNEX TO THE INTERNATIONAL SEARCH REPORT
ON INTERNATIONAL PATENT APPLICATION NO.

GB 8900320
SA 27811

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Patent document cited in search report	Publication date	Patent family member(s)		Publication date
EP-A- 0211587	25-02-87	JP-A-	62049244	03-03-87
EP-A- 0242527	28-10-87	JP-A-	62240864	21-10-87
EP-A- 0103426	21-03-84	US-A-	4447546	08-05-84
		JP-A-	59081560	11-05-84
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		JP-T-	58501481	01-09-83
		US-A-	4608344	26-08-86
EP-A- 0214768	18-03-87	JP-A-	62035246	16-02-87

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